

**Appendix 5 - Research Activity****1. Ionising radiation SPECT and CT RPMS 1975-8 and UCL 1978-80**

At the Royal Postgraduate Medical School, Hammersmith Hospital, with the MRC cyclotron unit, I used radioisotope images to measure lung function, and to tomographically image the liver. Radioactive gases from the MRC Cyclotron Unit were imaged using a gamma camera. I designed a CT machine<sup>1,2</sup> to image the heart. At UCL Medical physics I used one of the first CT machines (EMI 5005 whole body scanner) to measure muscle size<sup>3</sup> and composition in muscular dystrophy, and bone mineral content in osteoporosis.

**2. In-vivo NMR spectroscopy of neonates at UCL 1978-85**

The first NMR spectrometer capable of studying humans (neonatal brains and adult limb muscles) was installed at UCL medical physics by Oxford Instruments. I constructed the surface coil<sup>4</sup> for the first human brain spectra, collected from premature babies at University College Hospital<sup>5</sup>. I made the first measurements of metabolite concentration<sup>6,7</sup> *in vivo*, in rat brain and muscle. In the first issue of the new journal NMR in Biomedicine, my review on measuring metabolite concentrations was the opening article<sup>8</sup>.

**3. MS and permeability from Gd MRI contrast agent at IoN Queen Square 1985-99**

In 1985 I joined the new MS NMR Research Unit at Queen Square, where Multiple Sclerosis lesions could be visualised using the new NMR imaging technique. The total volume of MS lesion could be measured<sup>9</sup> and used as an indicator of disease severity and progression. The new contrast agent Gd-DTPA was being used to detect leakage in the blood-brain barrier (BBB) in MS lesions. I used dynamic MRI of Gd to measure BBB (capillary) permeability<sup>10,11</sup>. This consists of repeated imaging using a T<sub>1</sub>-weighted sequence, and measuring the time course of the uptake of Gd. A mathematical compartmental model is then fitted to give estimates of the permeability and extracellular space. Aspects of the model were refined<sup>12,13</sup>. This model was reconciled with others<sup>14,15</sup> and an international agreement was reached on interpretation and nomenclature<sup>16</sup>. The model has since been applied extensively in cancer<sup>17-19</sup>, to quantify tumour vascularity, and is now sometimes known as the 'Tofts model'. This measurement can be combined with blood volume<sup>20</sup>.

**4. Magnetisation Transfer (MT), diffusion and other new MR parameters 1995-2005**

The phenomenon of MT enables measurements to be made on normally invisible restricted protons located in cell structures. These are often more specific for biological change than conventional MRI. Initial measurements were with the Magnetisation Transfer Ratio, which at first showed large inter-centre variation<sup>21</sup>. The causes of differences between measurements made on different MRI scanners have now been analysed and largely removed, enabling multi-centre studies to be made<sup>22</sup>. A more fundamental way of measuring the properties of tissue (Quantitative MT) has been developed more recently<sup>23,24</sup>, where the fraction of restricted protons is obtained explicitly, and this shows promise in being more specific for biological change<sup>25</sup>. A 3D volume acquisition gives improved signal-to-noise ratio and spatial resolution<sup>26</sup>.

The diffusion of water is very sensitive to the presence or absence of biological barriers at the cellular level, and measurements of the apparent diffusion coefficient enable microscopic

biological changes to be detected<sup>27,28</sup> even though the spatial resolution of the MRI machine is about 1mm.

Blood flow can be measured accurately using arterial spin labelling<sup>29</sup>, and normal intra-subject variation can be observed<sup>30</sup>. In MS, acute lesions show increased blood flow<sup>31</sup>. There are a number of structural parameters which can be extracted from MRI images. These include the obvious ones such as size and volume, and the more subtle ones such as texture<sup>32</sup>. Histograms of large volumes of tissue are exquisitely sensitive to subtle changes in normal-appearing tissue<sup>33,34</sup> (after a common artefact in their generation had been solved<sup>35</sup>), and multi-centre performance can be good<sup>36</sup>.

## 5. Quantification - a new paradigm in MRI 1978-2005

After the initial successes in measuring metabolite concentration and capillary permeability, it was clear that a paradigm change in the way that MR machines are used was appropriate. A move from the *MRI-camera* to the *MR-scientific-instrument* would allow a whole range of quantities to be measured in the living body. There was increasing interest from clinicians (both in academia and pharmaceutical companies) in measuring the effects of disease and its progression, and the effects of drug treatments in clinical trials. The first book on the subject was designed, a range of international authors agreed to contribute, and in 2003 *Quantitative MRI: measuring changes caused by disease* was published by Wiley<sup>37</sup>. The reviews were excellent, it won the BMA Radiology book prize, and went paperback. ISMRM (the International Society for Magnetic Resonance in Medicine) asked for a course on the subject. A new topic in medicine had been born.

Individual patient treatment (for example in cancer) could include quantitative imaging to assess what type of treatment would be effective (e.g. chemotherapy, radiotherapy, surgery etc), and ongoing imaging to measure response to treatment (not only has the tumour decreased in size?, but also has it lost its ability to grow?) and whether an alternative was likely to be more suitable.

Many aspects of the physical MR instrument were understood and characterised. Phantoms (test objects) were developed<sup>38,39,40</sup>, and programs of Quality Assurance set up<sup>41,42</sup>. Image intensity nonuniformity was understood<sup>43,44</sup> and corrected<sup>45,46</sup>. Small objects can sometimes be characterised without partial volume error<sup>47</sup>. The factors which must be controlled in order to carry out multi-centre studies were identified<sup>22,48,49</sup>. Accurate ways of measuring MR parameters in the presence of the inevitable imperfections were developed<sup>50</sup>.

## 6. Quantitative applications in AD, epilepsy, gliomas, SLE and retina 1995-2005

With the success of the quantitative techniques, it became easier to interest clinicians outside MS in collaborating. The optimised techniques, with established reliability and normative data, could easily be used in other neurological diseases. On the new epilepsy imager, MT and the T<sub>2</sub> relaxation time were found to be abnormal<sup>51,52</sup>. In Neuropsychiatric SLE subtle changes in the MT properties of normal-appearing brain were seen<sup>53</sup>. Retinal disease could be characterised by the leakage of Gd from capillaries<sup>54</sup> and retinal oxygenation can also be measured noninvasively<sup>55,56</sup>. Recent work has shown that in gliomas the tumour type and prognosis can be predicted from the MRI Gd and diffusion behaviour. In Alzheimer's Disease the hippocampal restricted proton concentration decreases in line with cognitive function. Post-mortem studies of MS tissue<sup>57</sup> enable the relationship between MR and biological changes to be clarified.

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